Circular external fixator application for midshaft tibial fractures: Surgical technique

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Abstract
The use of fine wire circular external fixation has recently undergone a resurgence in popularity among orthopaedic trauma and reconstructive surgeons. Their modularity, biomechanical characteristics and minimally invasive application make these fixators indispensable for complex trauma and post-traumatic limb reconstruction. The application of these fixators is technically demanding and a steep learning curve exists. This article aims to provide a simplified, stepwise approach to the application of a circular external fixator to the tibia.

Key words: Ilizarov, circular external fixator, surgical technique

Introduction
Gavril Abramovich Ilizarov popularised the use of fine wire circular external fixators in Russia during the Cold War. Introduction to the West only came in 1981 after an Italian photojournalist, Carlo Mauri, was treated for a tibial non-union by Dr Ilizarov. In the following three decades we have seen a dramatic increase in the utilisation of fine wire external fixators, with a growing number of applications in elective and trauma orthopaedic surgery. The Ilizarov system, as well as the Ilizarov principles of distraction osteogenesis, has subsequently become indispensable for limb reconstruction surgery. Circular fixation has several advantages in the trauma setting, including the minimally invasive nature of application and the establishment of the optimal biomechanical milieu for fracture union. In this article we describe our surgical technique for applying a fine wire circular external fixator for a midshaft tibial fracture.

Biomechanical principles
Physiological loading of a fractured bone will cause deformation in three linear and three rotational dimensions. The resultant inter-fragmentary motion at the fracture site is therefore considered to be three-dimensional in nature. When an external fixator is used to immobilise a fracture the resultant stability can be conceptualised as the sum of the contributions from the external fixator and bone – the concept of shared stability.

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This overall stability will produce a degree of inter-fragmentary motion that is unique to each specific fracture-fixator configuration.

The biomechanical environment of the fracture site will influence both the pattern and rate of fracture healing. This environment is influenced by the mechanical properties of the external fixator, and can be reported in terms of axial stiffness, translational stiffness, and resistance to bending and torsion at the fracture site. Axial micromotion promotes bone regeneration while translational shear leads to the formation of fibrocartilage and predisposes to non-union. Bending micromotion can stimulate callus formation, but is more likely to lead to shear if the centre of rotation is not exactly at the centre of the fracture site.

The optimal external fixator would therefore promote a degree of axial micromotion while preventing excessive bending and translational shear.

Circular external fixators are fundamentally different from monolateral fixators. Through the use of tensioned fine wires as fixation elements, as opposed to half-pins, ring fixators are imparted with elastic properties and a low axial stiffness, while simultaneously preventing excessive bending and translational shear. Tensioned fine wires also contribute to the circular external fixator’s ability to exhibit increased axial stiffness with higher loads. This non-linear, load-dependent axial stiffness is similar to the viscoelastic properties of tendons and ligaments, and this biomechanical attribute has led to fine wire circular external fixators being described as the only form of ‘true biological fixation’. This biomechanical superiority along with their modularity and minimally invasive application make circular external fixators ideal for the management of complex trauma and limb reconstruction surgery.

In order to benefit from these circular external fixator characteristics, certain biomechanical principles must be adhered to:

Rings and ring blocks:
- Rings should be the minimum diameter that allows two finger breadths between the ring and skin surface.
- A ring-block should be used to stabilise each bone segment.
- Ring-blocks should consist of two rings and four connecting rods.
- Ring-blocks should have the maximum possible spacing between each ring. Rings that are spread more than 160 mm apart lead to torsional instability of that frame segment. When such a long spread is required, a ‘Dummy ring’ (interposed ring without fixation to bone) can be used to stabilise that frame segment.
- All rings should be assembled parallel to each other, and aligned perpendicular to the mechanical axis of the bone segment.

Wires and wire insertion:
- Each ring should have at least two tensioned fine wires, positioned as close to right angles to each other as possible.
- Wire insertion technique is crucial in order to prevent complications. Insertion must be along predetermined anatomical safe zones and with as low energy as possible.
- For adult lower limb trauma, 1.8 mm wires tensioned to 100–130 kg are required.

Surgical technique

Meticulous pre-operative surgical planning is essential with the use of circular external fixators. The modularity of ring fixator systems affords the user the ability to construct a specific external fixator configuration for each individual fracture pattern. This attribute is especially beneficial when dealing with complex fractures, but the process can be very time-consuming when done in theatre. We therefore advise that, after studying the fracture pattern, a custom external fixator is prebuilt for each case and sterilised fully assembled (Figure 1).

Essential to this technique is constructing a frame with two ring blocks, and the ability to adjust the distance between the ring blocks. When building our trauma frames we incorporate long threaded rods in one of the ring blocks (Figure 1). This allows intra-operative adjustment of the distance between the ring blocks, resulting in inter-fragmentary compression or distraction. During frame application, the frame is set at moderate distraction to facilitate fracture reduction.

The first few steps of the external fixator application are critical to fracture reduction. This involves application of the proximal and distal reference wires, which are inserted in close proximity to the joint capsules of the knee and ankle respectively. In order to avoid traversing the joint capsules, and eliminating the potential risk of septic arthritis, these wires should be placed outside the reflections of the joint capsules. For the knee and ankle joints, this is approximately 1.5 cm and 1.0 cm respectively.

Accurate placement of the reference wires, parallel to the knee and ankle joint lines, will address coronal plane angulation. The proximal reference wire is inserted transverse (in the coronal plane), and parallel to the tibial plateau articular surface / perpendicular to the proximal fragment mechanical axis (Figure 2). The prebuilt frame is applied to the limb, fixed to the wire, and the wire is tensioned. The distal reference wire is then inserted in the coronal plane, and parallel to the distal tibia articular surface / perpendicular to the distal fragment mechanical axis (Figure 3). Attaching and tensioning the distal reference wire to the distal ring will align the proximal and distal fragments in the coronal plane (Figure 4). It is important to ensure proper rotational alignment before attaching the distal reference wire.
Once coronal plane angulation is corrected, attention must be given to translation and angulation in the sagittal plane. This is addressed by the position in which the distal reference wire is attached to the frame. Due to gravity and patient positioning, the distal fragment will usually be translated posteriorly and angulated in recurvatum (Figure 5). Posterior translation of the distal fragment is corrected by attaching the distal reference wire in the anterior half of the ring and aligned with the knee in the coronal plane (Figure 6).

Coronal translation and sagittal angulation are the final displacements to be addressed. Firstly, coronal translation is corrected by sliding the fracture fragments along the reference wires until aligned (Figure 7). Sagittal angulation (Figure 6) is corrected by rotating the fracture fragments around the reference wires until alignment is restored (Figure 8). Rolled up towels will maintain this reduction until it can be stabilised with fixation to the middle two rings. This final position is maintained by adding fixation to the two middle rings.

Adding a second, tensioned wire to every ring on the frame completes the fixation. This wire can safely be placed parallel and deep to the anteromedial surface of the tibia (approximately 60° to the horizontal / transverse wire.) The final adjustment of the fixator is compression across the fracture site. This is accomplished by adjusting the distance between the proximal and distal ring blocks (Figure 9).

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The most common post-operative complication of circular external fixators is pin tract infection.\textsuperscript{16,20,21} The first step in preventing pin site infection is a meticulous insertion technique. Wire and pin insertion should be as low energy as possible, with minimum damage to the skin, soft tissue and bone. Following frame application, we advocate dressing pin sites with an alcoholic solution of chlorhexidine-soaked gauze.\textsuperscript{16,17,22} These dressings are left undisturbed for the first seven days, followed by twice daily cleaning with a chlorhexidine solution.\textsuperscript{16,27}
Conclusion

The surgical technique described in this article is simple, reproducible and effective. Accurate reference wires serve as the foundation for a successful frame application. Fracture reduction proceeds in a stepwise fashion, starting with coronal plane angulation and translation, followed by sagittal plane translation and angulation. Finally compression allows for accurate apposition of the fracture fragments. When these steps are followed meticulously it allows the surgeon the ability to obtain anatomical reductions for midshaft tibial fractures.

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