Introduction

Echocardiography remains the first line of imaging assessment for valvular heart disease (VHD) because of its wide availability, portability and low cost. Recent developments in real-time 3D echocardiography have improved the imaging of native valve anatomy and the quantification of valve geometry and function. Echocardiography, however, is often limited by the patient’s acoustic window. Also, inter-observer variation limits the assessment of changes in disease severity and progression.

In 2006, the American College of Cardiology acknowledged the increasing role that cardiovascular magnetic resonance (CMR) has to play in the assessment of patients with VHD, and gave CMR an ‘A’ appropriateness rating for ‘characterization of native and prosthetic cardiac valves – including planimetry of stenotic disease and quantification of regurgitation diseases’ and ‘patient(s) with technically limited images from echocardiograms or TEE’.

The superb spatial and temporal resolution of CMR, as well as its reproducibility and independence from patient body habitus and acoustic window, make it an excellent tool for not only diagnostic assessment but also follow-up of these patients to determine the optimal time for intervention. This article reviews the anatomy and pulse sequences used to assess these patients and provides an approach for CMR valvular assessment. In addition, it reviews the role of CMR in the assessment of patients with VHD.

Pulse sequences

For patients with VHD, start with a basic CMR protocol:

- axial black blood images of the thorax
- two-chamber cine steady state free precession (SSFP) images
- four-chamber cine SSFP images
- left ventricular outflow tract (LVOT) cine SSFP images
- short-axis cine SSFP images of the ventricles
- axial cine SSFP images through the valve.

After this, the protocol is tailored to the valve involved. For left-sided heart valves, phase contrast images should be added through the aorta. For right-sided heart valves, right ventricular outflow tract (RVOT) cine SSFP images and phase contrast images are added through the pulmonary artery.

When determining if the stenosis or pathology is at the level of the valve or subvalvular, as in cases involving the aorta and pulmonary valves, coronal images through the valve may also be helpful (Figure 1).

The two-chamber, four-chamber and LVOT cine images are useful to assess for mitral regurgitation. The axial cine images though the mitral valve give a good view of all the leaflets, allowing assessment of leaflet morphology.
Similarly, the four-chamber and axial cine images are useful to assess for tricuspid regurgitation. The four-chamber cine image also best depicts the attachment of the septal leaflet of the tricuspid valve for the assessment of Ebstein’s abnormality. For assessing leaflet morphology, the axial cine images through the tricuspid valve are most useful.

**Cardiovascular magnetic resonance in valvular heart disease**

The assessment of valves using CMR can be structured in the following way:

- normal anatomy
- valve morphology
- valve function
- ventricular function.

**Anatomy**

**Aortic valve**

The aortic valve is a tricuspid valve with three valve cusps: the right coronary cusp, the left coronary cusp and the non-coronary cusp (Figure 2a). Small spaces are seen between the attachments of the cusps to the aortic wall, called commissures (Figure 2b). On the coronal images of the aortic root the aortic cusps, the sinus of Valsalva and sinotubular junction can be assessed in plane (Figure 2c). The coronary arteries normally arise from the sinus of Valsalva below the level of the sinotubular junction.

**Mitral valve**

The mitral valve consists of leaflets (the anterior and posterior leaflets; Figure 3a), each of which can be divided into three
components. Each of the leaflets are attached to a papillary muscle via a tendinous cord (Figure 3b), and two sets of papillary muscles are seen on the short-axis images – the anterior lateral and the inferior medial papillary muscles.

Pulmonary valve
The pulmonary artery is the most anterior great vessel on the axial images. The pulmonary valve appears anatomically very similar to the aortic valve and also has three cusps: the anterior, left and right cusps (Figure 4).

Tricuspid valve
The tricuspid valve is a three-leaflet valve with an anterior, septal and posterior leaflet (Figure 5a). Each of these leaflets is attached to similarly named papillary muscles via tendinous cords (Figure 5b).

Valve morphology
Number of leaflets
Part of the morphological assessment of the cardiac valves is to assess the number of valve leaflets. Congenital leaflet number abnormalities are fairly uncommon and are most often in the aortic valve.

The most common leaflet abnormality of the aortic valve is a bicuspid aortic valve. The most common form of the bicuspid aortic valve is that of a valve with one raphe (Figure 6a) which is the result of fusion of two adjacent cusps. On rare occasions, the bicuspid valve is secondary to a bisinus valve, with only two sinuses of Valsalva and two cusps. No raphes are seen in these cases but the abnormality still results in the same characteristic ‘fish mouth’ opening of the valve (Figure 6b).

Leaflet number abnormalities in the other valves are extremely rare, but leaflets ranging from 2 to 5 have been described for the pulmonary and tricuspid valves.

Attachment abnormalities
The most common attachment abnormality of the valves is Ebstein’s abnormality, where there is apical displacement of the implantation of the septal leaflet of the tricuspid...
valve (Figure 7). The degree of apical displacement varies with Ebstein’s abnormality and is classified as abnormal if apical displacement of the septal leaflet of more than 8 mm/m² is present. This results in part of the right ventricle being incorporated into the right atrium and subsequently increases the right atrial size and decreases the functional right ventricle volume.

Leaflet integrity

The leaflets need to be assessed for tears, clefts or prolapses. Normally the flow jet from regurgitation secondary to ventricular dilatation is directed directly posteriorly. Tears and clefts can be acquired or congenital and are normally seen as an extra or eccentric flow jet arising from the leaflet (Figure 8).

Prolapse is seen as atrial displacement of the leaflets. The easiest way to assess this is to draw a line through the annulus and measure the distance from the line to the leaflet. If the displacement is more than 2 mm, it is in keeping with prolapse. An associated regurgitation jet is also normally seen.

With leaflet prolapse, as with tears and clefts, the flow jet is eccentric. In mitral valve prolapse, the jet is directed anteromedially towards the septum with prolapse of the posterior leaflet, and is postero-central or postero-lateral with anterior leaflet prolapse. In the instance of bi-leaflet prolapse, the flow jet is in a postero-medial direction (Figure 9).
Papillary muscle and tendinous cords

There is considerable variation in the number of tendinous cords normally seen attaching to each of the five papillary muscles, with an average of 12 tendinous cords per papillary muscle. The individual papillary muscles are normally the same thickness as the normal left ventricular myocardium.

The most common congenital abnormality of the papillary muscles is a single papillary muscle to which all the tendinous cords of the mitral valve attach (Figure 10), resulting in a ‘parachute’ mitral valve.9

Acquired abnormalities of the papillary muscles are, however, much more common. The most common primary tumour of the papillary muscles is fibroelastoma which may be situated...
on the papillary muscle or on the tendinous cords. However, more common than primary tumours of the papillary muscles is the local invasion or involvement of the papillary muscles owing to direct extension of left ventricular myocardial disease, tumours (Figure 11) or ischaemic scarring.

Valvular function

SSFP and gradient echo sequences can visualise flow disturbances caused by valvular stenosis or regurgitation on the basis of signal loss owing to dephasing of moving protons. This helps to locate the jet for the dephasing origin and direction. Although SSFP imaging provides better visualisation of valve anatomy, it is less sensitive to phase disturbances than gradient echo sequences, making it easier to miss or underestimate severe regurgitation. 10

Phase contrast sequences are also used for valvular assessment, particularly of the aortic and pulmonary valves. These sequences are based on the accumulated phase of moving protons and are used to measure the peak velocity, stroke volume, and regurgitation fraction in a vessel. These images needs to be acquired directly perpendicular to the vessel for accurate measurements (Figure 12). Valvular stenosis is seen as increased signal in the region of the flow jet (Figure 13).

Stenosis

In patients with valvular stenosis, dephasing or a flow jet can be seen distal to the valve (Figure 14). Smaller openings,
characteristic of severe disease, cause more dephasing and a
darker jet is seen. The phase contrast images in severe stenosis
will also demonstrate higher velocities, which will be seen as
an area of complete signal loss owing to aliasing if it is above
the programmed maximum velocity. This will result in an
underestimation of the peak velocity as velocities higher than
the programmed maximum velocities cannot be detected. In
these instances, the programmed maximum velocity needs to
be adjusted until the aliasing artefact disappears. The area of
maximum opening of the valve can also be measured on the
axial SSFP cine images through the valve (Figure 15).

Regurgitation
Valvular regurgitation is seen as dephasing or as a flow jet
proximal to the valve (Figure 16). With regurgitation, more
severe disease results in a large opening which causes less
dephasing and thus results in a less obvious jet.

Aortic and pulmonary valve regurgitation is normally
measured directly with phase contrast images. By drawing a
region of interest in the vessels, the forward volume and
regurgitation volume can be measured and used to calculate
the regurgitation fraction (regurgitation volume/forward
volume × 100).\textsuperscript{11}

Normally, phase contrast images are not used to directly assess
the regurgitation fraction for the mitral and tricuspid valves.
For these two valves, the regurgitation fraction, as measured
on the phase contrast images of the aorta and pulmonary
arteries, is calculated using the ventricular stroke volume and
the aortic and pulmonary forward volumes respectively:

\begin{itemize}
  \item mitral regurgitation = left ventricular stroke volume –
aortic forward stroke volume\textsuperscript{10}
  \item tricuspid regurgitation = right ventricular stroke volume –
pulmonary forward stroke volume.\textsuperscript{10}
\end{itemize}

Ventricular function
CMR is not only an excellent modality for assessing the cause
of valvular disease and quantifying the severity of the
disease, but it has also been shown to be the most reliable
modality to assess the consequences of the VHD.\textsuperscript{12} The
consequences of VHD are assessed by looking at the
ventricular size and function. Because of the reproducibility
of CMR, it now forms an integral part in the assessment of
these patients for valve replacement surgery.\textsuperscript{12}
Conclusion

CMR plays an increasingly important role in the pre-surgical assessment of patients with VHD. CMR is particularly useful to assess valvular anatomy and function, quantify the severity of the disease, as well as assess the sequelae of VHD, with accurate assessment of ventricular size and function.

Competing interests

The author declares that she has no financial or personal relationships which may have inappropriately influenced her in writing this article.

References